

1 PREPARED FOR SUBMISSION TO JINST
2 12TH INTERNATIONAL CONFERENCE ON POSITION SENSITIVE DETECTORS
3 12-17 SEPTEMBER 2021
4 UNIVERSITY OF BIRMINGHAM, BIRMINGHAM, U.K.

5 The Bergen proton CT system

6 M. Aehle,^p J. Alme,^a G.G. Barnaföldi,^c T. Bodova,^a V. Borshchov,^l A. van den Brink,^d M.
7 Chaar,^a V. Eikeland,^{a,1} G. Feofilov,^q C. Garth,^o N.R. Gauger,^p G. Genov,^a O. Grøttvik,^a H.
8 Helstrup,^e S. Igolkin,^q R. Keidel,^k C. Kobdaj,^m T. Kortus,^k V. Leonhardt,^o S. Mehendale,^a
9 R.N. Mulawade,^k O.H. Odland,^{a,b} G. O'Neill,^a G. Papp,^g T. Peitzmann,^d H.E.S. Pettersen,^b P.
10 Piersimoni,^a M. Protsenko,^l M. Rauch,^a A. Ur Rehman,^a M. Richter,^h D. Röhrich,^a J.
11 Santana,^k A. Schilling,^k J. Seco,^{i,j} A. Songmoolnak,^{a,m} J.R. Sølve,^{a,f} G. Tambave,^a I.
12 Tymchuk,^l K. Ullaland,^a M. Varga-Köfaragó,^c L. Volz,^{i,j} B. Wagner,^a S. Wendzel,^k A. Wiebel,^k
13 R. Xiao,^{a,n} S. Yang,^a H. Yokoyama,^d S. Zillien,^k

14 on behalf of the Bergen pCT collaboration

15 ^aDepartment of Physics and Technology, University of Bergen, Bergen, Norway

16 ^bDepartment of Oncology and Medical Physics, Haukeland University Hospital, Bergen, Norway

17 ^cDepartment for Theoretical Physics, Heavy-Ion Research Group, Wigner RCP of the Hungarian Academy
18 of Sciences, Budapest, Hungary

19 ^dInstitute for Subatomic Physics, Utrecht University/Nikhef, Utrecht, Netherlands

20 ^eDepartment of Computing, Mathematics and Physics, Western Norway University of Applied Science,
21 Bergen, Norway

22 ^fDepartment of Electrical Engineering, Western Norway University of Applied Sciences, Bergen, Norway

23 ^gInstitute for Physics, Eötvös Loránd University, Budapest, Hungary

24 ^hDepartment of Physics, University of Oslo, Oslo, Norway

25 ⁱDepartment of Biomedical Physics in Radiation Oncology, German Cancer Research Center, Heidelberg,
26 Germany

27 ^jDepartment of Physics and Astronomy, Heidelberg University, Heidelberg, Germany

28 ^kCenter for Technology and Transfer (ZTT), University of Applied Sciences Worms, 67549 Worms, Germany

29 ^lResearch and Production Enterprise "LTU", Kharkiv, Ukraine

30 ^mInstitute of Science, Suranaree University of Technology, Nakhon Ratchasima, Thailand

31 ⁿCollege of Mechanical and Power Engineering, China Three Gorges University, Yichang, China

32 ^oChair for Scientific Visualization Lab, Technische Universität Kaiserslautern, Kaiserslautern, Germany

33 ^pChair for Scientific Computing, Technische Universität Kaiserslautern, Kaiserslautern, Germany

34 ^qSt. Petersburg University, St. Petersburg, Russia

35 E-mail: viljar.eikeland@uib.no

¹Corresponding author.

36 ABSTRACT: The Bergen proton Computed Tomography (pCT) is a prototype detector under con-
37 struction. It aims to have the capability to track and measure ions' energy deposition to minimize
38 uncertainty in proton treatment planning. It is a high granularity digital tracking calorimeter, where
39 the first two layers will act as tracking layers to obtain positional information of the incoming parti-
40 cle. The remainder of the detector will act as a calorimeter. Beam tests have been performed with
41 multiple beams. These tests have shown that the ALPIDE chip sensor can measure the deposited
42 energy, making it possible for the sensors to distinguish between the tracks in the Digital Tracking
43 Calorimeter (DTC).

44 Contents

| | | |
|----|-------------------------------|----------|
| 45 | 1 Introduction | 1 |
| 46 | 2 Design | 1 |
| 47 | 3 Simulation | 2 |
| 48 | 4 Experimental Results | 3 |
| 49 | 5 Conclusion | 3 |

50 1 Introduction

51 Hadron therapy has become a widely accepted treatment form for malignant tumours in the last 20
52 years. It is a method that takes advantage of the concentrated dose delivery to a confined area for
53 charged particles. Proton Computed Tomography (pCT) is an imaging technique used in diagnostics
54 to directly reconstruct a charged particle's relative stopping power (RSP) as it traverses the object
55 of interest. This allows for a reduction in uncertainty, which in turn reduces the dose delivered to
56 healthy tissue during the treatment phase. The Bergen pCT collaboration is constructing a Digital
57 Tracking Calorimeter (DTC) to accurately track and determine individually charged particles' range
58 and inherent energy. As a particle traverses the detector, it will deposit energy in the sensitive layers
59 and thus produce a 3D digital hit map along its path. Most pCT scanners utilize both a front-tracker
60 and a rear-tracker in the imaging process. The Bergen pCT, however, is designed as a multilayered
61 sandwich structure without a front tracker. Positional information about the incoming particles will
62 be obtained from beam optics. Thus the Bergen pCT can be classified as a single-sided tracker
63 system [1].

64 2 Design

65 The pCT is composed of 43 layers in total, where each detector layer is electrically identical with 108
66 ALPIDE chip sensors per layer. The first two layers will act as tracking layers to obtain positional
67 information about the incoming particle. The 41 subsequent layers will act as a digital calorimeter
68 composed of CMOS pixel sensors. Each Digital Tracking Calorimeter (DTC) layer is constructed
69 similarly, albeit with minor differences between the tracking and calorimeter layers. The ALPIDE
70 chip sensor is a monolithic active pixel sensor. It is manufactured utilizing the 180 nm CMOS
71 Imaging Sensor process by TowerJazz Semiconductor. The ALPIDE chip ($30 \times 15 \text{ mm}^2$) contains a
72 matrix of 1024×512 pixels. Each pixel can amplify, discriminate, and shape the incoming signal,
73 and they measure $\approx 27 \times 29 \mu\text{m}^2$ in size. The high granularity provided by the ALPIDE chip allows
74 for simultaneous tracking of multiple particles [2].

75

76 Nine ALPIDE sensor chips are single-point tape-automated bonded to a flex cable known as a
77 *string*. Three strings together on a 1mm thick aluminium plate constitute a slab. A slab can either
78 be top or bottom. A top and a bottom slab together create a half layer, shown in Figure:1a. A half
79 layer is not capable of covering the entire area because of the non-sensitive part of the flex cables.
80 A complete layer is constructed by utilizing two half layers facing each other with alternating chip
81 positioning to cover the entire area. The two half layers facing each other are illustrated in Figure:1b.
82 The layout of the calorimeter layers of the pCT is as described above. They will be mounted with
83 100 μm thick ALPIDE chips, and 3.5 mm aluminium plates will be used as absorber material
84 between the layers. For the tracking layers, it is desirable to minimize the non-sensor material.
85 To achieve this, 50 μm thick ALPIDE chips will be mounted on $\approx 300 \mu\text{m}$ thick carbon-epoxy
86 sandwich sheets, covering an area of $200 \times 290 \text{ mm}^2$. Each sheet is composed of three layers of
87 carbon paper and two layers of carbon fleece. The final prototype will have a size of $27 \times 16.6 \text{ cm}^2$,
88 large enough to image a human head.

89

90 The ALPIDEs mounted on a string share the same clock and slow control signals. Each ALPIDE
91 sensor has its individual 1.2 Gbit/s LVDS data line. Each layer is connected to a custom-made
92 transition card (TC), an intermediate between the ALPIDE chip sensors and the readout electronics.
93 Each layer has a dedicated pCT readout Unit (pRU) based on a Xilinx Kintex Ultrascale FPGA, and
94 the communication between the pRU and the TC is via twelve Samtec FireFly connectors [1].

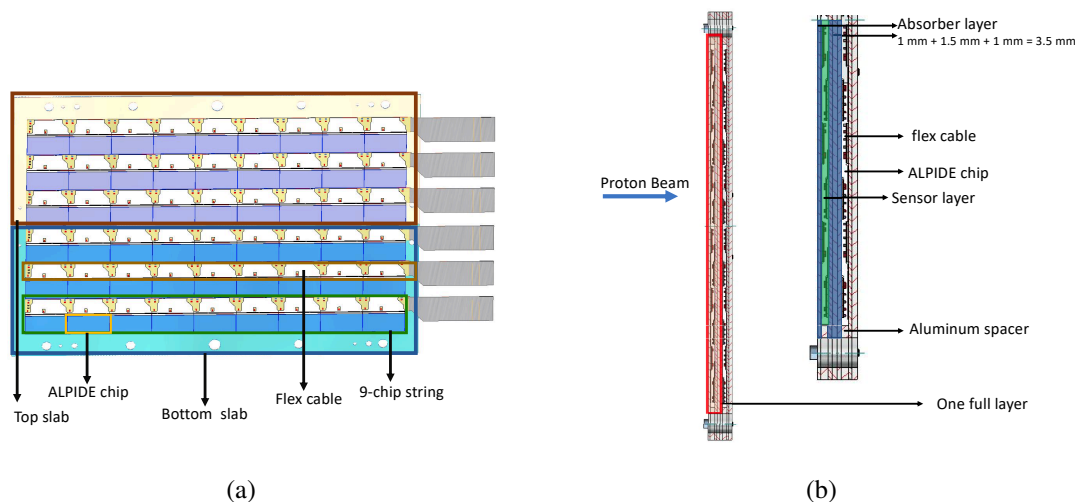


Figure 1: (a) Half layer consisting of a top slab and a bottom slab [1]. (b) Schematic side view of two layers in the calorimeter(left), and half layer with details(right) [1].

95 3 Simulation

96 Different views of a head phantom reconstructed with the modelled setup can be observed in Figure
97 2a. The image shows that the different salient structures in the head are well distinguishable. A
98 detailed description of the simulation for the Bergen pCT scanner can be found in [1].

99 4 Experimental Results

100 The ALPIDE chip sensor has been tested in multiple beam environments allowing for the charac-
101 terization of the ALPIDE chip to understand the behaviour of the final pCT system. In Figure 2b
102 the cluster size measured by the ALPIDE as a function of the deposited energy in the epitaxial
103 layer of the ALPIDE is presented. It can be observed that there is a clear correlation between the
104 deposited energy and the cluster size which will be used to give a more accurate description of the
105 range of an incoming particle in the DTC. The capability of the ALPIDE to distinguish between the
106 deposited energies of the incoming particles also allows for the identification of different particle
107 species. This will allow the DTC to function as a continuous tracking device capable of identifying
108 interactions, such as hadronic processes or Coulomb scattering, as these will produce different
109 cluster distributions in the DTC. In turn, this identification of particles will provide a filter allowing
110 for the possibility to distinguish between a primary and a secondary particle, which will be helpful
111 for the reconstruction [1].

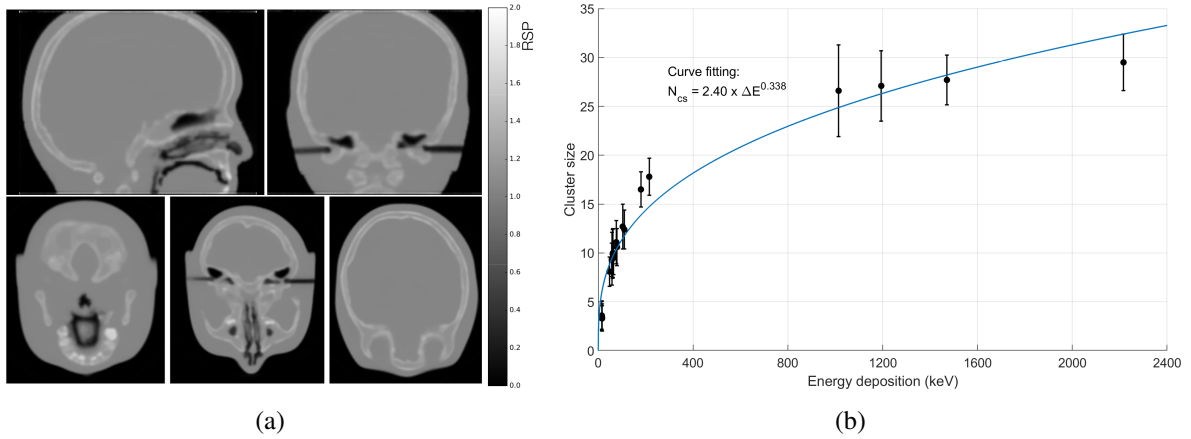


Figure 2: (a) From top left to bottom left clockwise: Sagittal, coronal, and three axial views of a full pCT reconstruction of the simulated head phantom in the modeled setup [1]. (b) Cluster size as a function of the energy deposition in the epitaxial layer of the ALICE pixel detector (ALPIDE) chip. The energy deposition was evaluated through MC simulation, the cluster sizes are obtained from multiple beam experiments [1]

112 5 Conclusion

113 The Bergen pCT scanner has shown a capability of acting as a high granularity DTC, functioning
114 both as a tracking device and an energy/range detector. Designing the system as a single-sided
115 tracker system allows it to be operated with a higher particle rate during the imaging process. The
116 design reduces both the complexity and the cost of the system compared to a two-sided detector
117 system. The prototype is built with scalability in mind, allowing for the possibility of future system
118 upgrades. The final prototype is expected to be installed in medical facilities by 2024 [1].

119 **References**

120 [1] J. Alme et al. *A High-Granularity Digital Tracking Calorimeter Optimized for Proton CT*, *Frontiers* **8**
121 (2020) 460.

122 [2] M. Mager *ALPIDE, the monolithic active pixel sensor for the ALICE ITS upgrade*, *Nucl Instrum*
123 *Methods Phys Res B* **824** (2016) 434-438.